Intrinsic Activated Microglia Map to the Peri-infarct Zone in the Subacute Phase of Ischemic Stroke

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**Background and Purpose** — Microglial activation is an important component of the neuroinflammatory response to ischemic stroke. Experimental studies have outlined such patterns temporally and spatially. In vivo studies in stroke patients have relied on positron emission tomography and (R)-PK11195, a ligand that binds peripheral benzodiazepine binding sites. In this study we sought to establish temporal and spatial patterns of microglial activation in ischemic stroke with particular emphasis on a defined peri-infarct zone.

**Methods** — Using this technique, we studied carotid territory ischemic stroke patients in 3 time windows up to 30 days after ictus. Controls were studied in a single session. [11C](R)-PK11195 injection was followed by 3-dimensional acquisition over 60 minutes. Cerebral blood volume (CBV) was measured afterward with the use of standard C 15O paradigms. Analysis employed the reference tissue model in which ipsilateral cerebellum was used to generate parametric binding potential maps corrected for CBV. Data were coregistered to T1-based MRI. Using control data to identify 99% confidence limits, a region of interest analysis was applied to identify significant binding in core infarction, contralateral hemisphere, and within a defined peri-infarct zone.

**Results** — Four patients (mean age, 66 years) were imaged across 9 sessions. Four age-matched controls were studied. Within this model, ipsilateral cerebellum was validated as a reference tissue. With the use of control-derived confidence limits and correction for CBV, significant binding potential rises were identified beyond 72 hours and extending to 30 days in core infarction, contralateral hemisphere, and peri-infarct zone.

**Conclusions** — In ischemic stroke patients, minimal activation of microglia is seen before 72 hours. Beyond this, binding potential rises in core infarction, peri-infarct zone, and contralateral hemisphere to 30 days. This may represent a therapeutic opportunity that extends beyond time windows traditionally reserved for neuroprotection. *(Stroke, 2006;37: 1749-1753.)*

Key Words: inflammation | microglia | positron emission tomography | tomography, emission computed

There is strong evidence that neuroinflammation contributes to the pathophysiology of cerebral ischemia and neuronal cell death.1 A consistent component of this process is recruitment and activation of microglia that produce neurotoxins such as interleukin-1β (IL-1β).2 IL-1β in turn promotes neuronal cell death by several mechanisms, including apoptosis.3 Much of this evidence has been obtained from experimental stroke models, although difficulty remains in extrapolation to the clinical setting.4 In rat middle cerebral artery (MCA) occlusion models, microglial activation extends beyond core infarction and could contribute to peri-infarct neuronal death.5,6 Comparatively little is known regarding whether strategies that seek to downregulate these processes are likely to provide benefit. In fact, we still do not know whether activated microglia can be demonstrated in peri-infarct areas in clinical stroke, particularly in tissue that may contribute to infarct expansion and poor outcome. Furthermore, we have no clear data on the temporal pattern of microglial activation in this setting. Such information can be obtained only if we have methods of imaging microglial activation in vivo.

The enantiomer (R)-PK11195 (1-2-chlorophenyl-N-methyl-N-1-methyl-propyl-3-isouqinolone carboxamide) labeled with 11C provides a positron emission tomography (PET) ligand to investigate the role of activated microglia in acute stroke. (R)-PK11195 binds to the peripheral benzodi-
aezepine binding site that is abundant on brain-derived activated microglia. After permanent MCA occlusion in rats, markers of microglial activity increase progressively up to 8 days and extend to 16 days, and binding is observed both in areas of infarction and beyond as defined by histological criteria. Such binding has been shown to be minimal in normal brain but significantly increased in areas of neuronal damage or inflammation. Similar evidence of microglial activation can be found with the use of [11C](R)-PK11195 PET in primate models of stroke, in both areas of infarction and peri-infarct tissue. However, although some clinical PET studies have examined the PK11195 binding after stroke, most patients have been studied on a single occasion, with some limited longitudinal data and information on the spatiotemporal evolution of the microglial response. Few studies have reported PK binding data coregistered with structural imaging such as MRI.

The purpose of this study was to investigate the temporal characteristics of PK binding with serial imaging in the first month after acute ischemic stroke. Our hypothesis, based on the animal literature, was that microglial activity would be present in the subacute phase and that such activity would map to peri-infarct zones, coinciding with areas that are commonly thought of as penumbra.

**Subjects and Methods**

Patients with clinically defined MCA territory ischemic stroke were studied sequentially within 3 time windows: ≤72 hours, 7 to 14 days, and 25 to 30 days (sessions 1 to 3, respectively). Age-matched healthy volunteers were imaged on a single occasion. Exclusion criteria for both patients and volunteers included benzodiazepine exposure within 72 hours and other forms of cerebral pathology. Written informed consent was obtained from all patients and volunteers in accord with protocols approved by the Local Research Ethics Committee and the Administration of Radioactive Substances Advisory Committee.

PET studies were performed sequentially on a GE Advance scanner. After acquisition of an attenuation scan, emission data were acquired for 60 minutes after the intravenous injection of ~250 MBq of [11C]PK11195 (±18.5 GBq/μmol specific activity at injection). Approximately 60 minutes after the injection of [11C]PK11195, 750 MBq of C15O was administered via nasal prongs over 1 minute, and emission data were acquired over the subsequent 5 minutes to quantify cerebral blood volume (CBV). Data were acquired in 3-dimensional mode with corrections for randoms, dead time, normalization, scatter, attenuation, and sensitivity. Total radiation dose per combined session amounted to 2.4 mSv.

Whenever possible, back-to-back T1 coregistration sequence and T2 MRI sequences were performed (Bruker). PET images were coregistered and resliced to the T1-weighted MRI with the use of the mutual information algorithm in SPM2 (Members and Collaborators, 2003). Quantification of [11C]PK11195 binding was made in defined regions of interest on parametric maps of binding potential.

PK parametric binding potential maps were obtained with the use of the simplified reference region (ipsilateral cerebellum) model implemented in the Receptor Parametric Mapping (RPM) software. We were concerned that the calculated binding potential would be contaminated by residual intravascular [11C]PK11195 activity that would vary with CBV in the presence of ischemia. The technique used to correct the PK PET data for CBV is described elsewhere. We measured [11C]PK11195 activity in a vascular region of interest (ROI) defined on the superior sagittal sinus on the C15O scan to obtain a measure of tracer activity in blood. Parametric CBV images were obtained from the C15O emission data with the use of standard kinetic models as described elsewhere. These were then used, along with the knowledge of vascular tracer activity, to correct images for residual contamination on a voxel basis (Figure 1). Two-tailed paired sample t tests were used to test for core stroke ROI-based differences in binding potential with and without CBV correction.

PET images and T2-defined structural core infarct ROIs were coregistered to the chronic T1-weighted images with the use of the vtkCISG software package (Computational Imaging Science Group, 2002). ROIs were defined for core infarct, patient reference tissue (ipsilateral cerebellum), and cerebellum for controls. Core infarct ROI was flipped by symmetry onto the unaffected hemisphere (termed mirror ROI) to allow comparison of findings in the infarcted tissue with those of contralateral homologous territory. MCA ROI was defined in each subject according to previously defined templates and projected onto the subject’s normalized binding potential map. Thereafter, each subject’s binding potential map was spatially normalized to a T1 template in SPM2 to obtain normalization parameters.

Our choice of reference tissue was dictated by concerns regarding the effects of cerebellar diaschisis. To assess the impact of this phenomenon, linear regression analysis was performed between the individual cerebellar time-activity curves (TACs) of the patients and the mean cerebellar TACs of the controls. To evaluate the suitability of a patient’s ipsilateral cerebellum as a reference tissue, comparisons were performed with the use of χ² tests between the TACs obtained from the cerebellar region of patients and those obtained from the control subjects. We used the Student t test to compare CBV values between patients and controls. Statistical significance was accepted if probability value was <.05.

We used the MCA ROI defined above to identify the CIs for PK binding potential values in the normal voxels in control subjects. The 99% upper confidence limit for normal PK binding potential was defined by the 8 MCA ROIs obtained from 4 controls subjects with the use of a 1-tailed t test. We wished to define a peripheral ROI that comprised those parts of the MCA territory that were not involved by the infarct. To avoid contamination of this peripheral ROI by infarcted tissue, we dilated the core infarct ROI by 2 PET spatial resolutions to form a “dilated core” ROI. As a marker of the peri-infarct zone, the dilated core ROI was subtracted from the MCA ROI to produce the peripheral ROI (Figure 2). The number of total voxels in an ROI (Nt) and the number of voxels in which PK binding potential intensities were greater or equal to the upper limit of the 99% CI of PK binding potential values from control ROIs (Nt,UL) were measured. In ipsilateral and mirrored peripheral ROIs, ratios of Nt,UL/Nt were calculated. Ipsilateral peripheral ROI values for Nt,UL/Nt were

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**Figure 1.** Schematic outlining procedure of generating PK binding potential parametric maps based on CBV correction. RPM indicates regional parametric mapping; CO, carbon monoxide.
compared with values from dilated core and mirrored ROI values on
a sessional basis with the use of a paired sample $t$ test.

## Results

### Patients

Four patients (3 male, 1 female) were imaged in a total of 9
sessions. Patient data are given in Table 1. Four age-matched
healthy volunteers (aged 64±5 years) were imaged on a
single occasion.

### Cerebellar TACs

There was a high degree of correlation between the mean
TAC in control cerebellar ROIs and that obtained from all
ipsilateral patient cerebellar ROIs ($r=0.95$ to 0.99). However,
the TAC from the contralateral cerebellar ROI was signifi-
cantly different from the mean control TAC for 2 patient
sessions. Patient data are given in Table 1. Four age-matched
healthy volunteers (aged 64±5 years) were imaged on a
single occasion.

### Corrected PK Binding Potential Maps

A 99% upper limit of 0.295 was defined for binding potential
with and without CBV correction were
not observed in patients ($P=0.48$) (Table 2). Mean $N_{iso}/N_T$
ratios from dilated core ROIs and ipsilateral and contralateral
peripheral ROIs are shown in Figure 3. Mean ipsilateral
values of $N_{iso}/N_T$ were not significantly greater than con-
tralateral values on a paired sessional basis ($P=0.57,
P=0.24$, and $P=0.43$ for sessions 1, 2, and 3, respectively).
Sessional differences between ipsilateral mean binding poten-
tial in dilated core versus peripheral ROI approached
significance in session 2 only ($P=0.27$, $P=0.09$, and $P=0.3$
for sessions 1, 2, and 3, respectively). Images from patient 1
are presented in Figure 4 as an illustration.

## Discussion

This image-based study confirms the effective use of PET
with the ligand (R)-PK11195 in the study of in vivo spatial and
temporal patterns of intrinsic microglial activity in
subacute ischemic stroke patients. This study is the first to
sequentially and quantitatively study such patterns within this
time frame and to do so with the use of correction for CBV.

### Table 2. Mean PK Binding Potential (Unitless) in Core Stroke ROI With and Without CBV Correction

<table>
<thead>
<tr>
<th>Patient No.</th>
<th>Age, y</th>
<th>Vascular Territory</th>
<th>Admission NIHSS Score</th>
<th>Combined PET and MRI Image Time, d</th>
<th>PK Binding Potential Without CBV Correction</th>
<th>PK Binding Potential With CBV Correction</th>
<th>Absolute Change (% Change)</th>
</tr>
</thead>
<tbody>
<tr>
<td>P1/S1</td>
<td>43</td>
<td>Left MCA</td>
<td>19</td>
<td>2, 13, 30</td>
<td>0.15±0.17</td>
<td>-0.17±0.18</td>
<td>-0.02 (-13)</td>
</tr>
<tr>
<td>P1/S2</td>
<td>36</td>
<td>Left MCA</td>
<td>13</td>
<td>2, 8, 25</td>
<td>2.68±0.51</td>
<td>3.07±0.67</td>
<td>0.39 (13)</td>
</tr>
<tr>
<td>P1/S3</td>
<td>31</td>
<td>Left MCA</td>
<td>12</td>
<td>3</td>
<td>0.69±0.4</td>
<td>0.75±0.48</td>
<td>0.07 (9)</td>
</tr>
<tr>
<td>P2/S1</td>
<td>70</td>
<td>Left MCA</td>
<td>13</td>
<td>2, 8, 25</td>
<td>-0.09±0.11</td>
<td>-0.08±0.15</td>
<td>0.01 (11)</td>
</tr>
<tr>
<td>P2/S2</td>
<td>26</td>
<td>Left MCA</td>
<td>13</td>
<td>3</td>
<td>0.26±0.24</td>
<td>0.24±0.26</td>
<td>-0.02 (-8)</td>
</tr>
<tr>
<td>P2/S3</td>
<td>77</td>
<td>Left MCA</td>
<td>11</td>
<td>2, 10</td>
<td>0.25±0.23</td>
<td>0.18±0.24</td>
<td>-0.07 (-28)</td>
</tr>
<tr>
<td>P3/S1</td>
<td>75</td>
<td>Left MCA</td>
<td>11</td>
<td>2, 10</td>
<td>-0.09±0.14</td>
<td>-0.07±0.14</td>
<td>0.02 (11)</td>
</tr>
<tr>
<td>P4/S1</td>
<td>75</td>
<td>Left MCA</td>
<td>11</td>
<td>2, 10</td>
<td>-0.14±0.34</td>
<td>-0.16±0.2</td>
<td>-0.02 (-14)</td>
</tr>
<tr>
<td>P4/S2</td>
<td>75</td>
<td>Left MCA</td>
<td>11</td>
<td>2, 10</td>
<td>0.24±0.22</td>
<td>0.20±0.26</td>
<td>-0.04 (-17)</td>
</tr>
</tbody>
</table>

Values are mean±1SD. Shown are patients (P) 1 to 4, sessions (S) 1 to 3,
and absolute and percent differences; $P=0.48$. 

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**Figure 2.** Schematic demonstrating defined ROIs (core, dilated core, peripheral) and MCA used in the image analysis.
Although correction for CBV did not significantly influence binding potential overall, given the plasma binding profile of PK11195, it remains likely that wide variations in CBV may influence local binding potential patterns. We have additionally validated the use of ipsilateral cerebellum within the well-established reference tissue model. This model can be used to quantify peri-infarct microglial activation beyond time windows traditionally reserved for neuroprotection.

Dependent on an experimental ischemic model, PK binding is evident from day 1 and may persist until day 16, and this can be confirmed histologically. Our data are broadly consistent with this time scale. The data on the temporal characteristics of the response show minimal binding within 72 hours, rising significantly within a week before some reduction by weeks 3 to 4. Spatially, binding remains high within core but appears not to extend to peri-infarct zones until 7 to 10 days. Remote microglial activation extends to contralateral hemisphere at these later time points. In patient-based imaging studies, nonsequential data have been collected at later time points up to 150 days after stroke. Here areas of PK binding can be found extending beyond the infarct site into connected areas of the hemisphere and contralateral thalamus. This is thought to represent Wallerian degeneration as a consequence of focal damage. We found some evidence of this within our mirrored ROIs, primarily at later time points. It remains to be established whether these remote phenomena are related to diaschisis or have other functional significance.

A comparison of these data with an MR-based study using supermagnetic iron oxide particles suggests hematogenous uptake of macrophages within parenchyma within a similar time frame but independent of blood-brain barrier function. It is generally thought that posts ischemic inflammation contributes to ischemic damage by a multitude of mechanisms. The benefi-
cial effects of such a cellular inflammatory response remain unknown but should not be dismissed. Activated microglia possess the potential to produce neurotoxins (including reactive oxygen species and toxic prostanoids) in addition to apoptotic agents such as IL-1β. In this small study, it is not possible to say whether the magnitude of the microglial response varies according to lesion size or ischemic severity. Correlation with final infarct volume and outcome also remains to be established. A recent study of neutrophil migration in ischemic stroke suggests that there is a heterogeneous response across ischemic strokes of similar type, of which microglia appear to form only a part. Given the ongoing paucity of effective neuroprotective strategies in stroke, the detection of microglial activity at later time points when patients present to physicians may provide a target for novel therapeutic agents designed to limit late neuronal damage and improve outcome. Such strategies should be undergo trials alongside existing treatments aimed at restoration of cerebral blood flow, in addition to well-accepted secondary prevention management.

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