Cortical Neuromodulation Modifies Cerebral Vasomotor Reactivity

Fabrizio Vernieri, MD; Giovanni Assenza, MD; Paola Maggio, MD; Francesco Tibuzzi, MD; Filippo Zappasodi, PhD; Claudia Altamura, MD; Marzia Corbetto, MD; Laura Trotta, MD; Paola Palazzo, MD; Matilde Ercolani, TNP; Franca Tecchio, PhD; Paolo Maria Rossini, MD

Background and Purpose—Cerebral vasomotor reactivity (VMR) is a capability of cerebral vessels to dilate in response to hypercapnia. Transcranial direct current stimulation (tDCS) effects on cerebral hemodynamics have been poorly studied. Anodal tDCS (A-tDCS) on primary motor cortex (M1) increases its excitability, whereas cathodal (C-tDCS) produces opposite effects. Because A-tDCS of M1 facilitates motor learning, it was tested in stroke rehabilitation and had promising results. However, tDCS effects on cerebral hemodynamics have not been studied. Cerebral tDCS increased VMR by 0.8%/mm Hg CO2 bilaterally and reduced LFNreact, whereas cathodal tDCS decreased VMR by 3.4%/mm Hg CO2 bilaterally and increased LFNreact.

Conclusions—Cerebral VMR is modified by tDCS. Based on the consensual changes with heart rate variability, we can hypothesize that the sympathetic nervous system could modulate the bihemispheric modification of VMR. Further studies are needed to confirm this hypothesis. (Stroke. 2010;41:2087-2090.)

Key Words: cerebral hemodynamics ■ heart rate variability ■ stroke ■ transcranial direct current stimulation ■ transcranial Doppler

Transcranial direct current stimulation (tDCS) can modulate brain function through a focal and prolonged cortical polarization shift. Anodal tDCS (A-tDCS) on primary motor cortex (M1) increases its excitability, whereas cathodal (C-tDCS) produces opposite effects. Because A-tDCS of M1 facilitates motor learning, it was tested in stroke rehabilitation and had promising results. However, tDCS effects on cerebral hemodynamics have not been studied. Cerebral tDCS increased VMR by 0.8%/mm Hg CO2 bilaterally and reduced LFNreact, whereas cathodal tDCS decreased VMR by 3.4%/mm Hg CO2 bilaterally and increased LFNreact.

Evaluation Before tDCS

Electrocardiographic signals were recorded throughout the experiment to assess heart rate variability (HRV), ie, the variability of the interval between consecutive heart beats. Transcranial Doppler examination was performed as described elsewhere. Mean flow velocity (MFV) in the middle cerebral arteries was recorded at rest condition (MFV baseline) and after the inhalation of a mixture of 7% CO2/air (MFV CO2). VMR values were obtained according to the formula:

$$VMR = \left( \frac{MFV_{CO2} - MFV_{Baseline}}{MFV_{Baseline}} \right) \cdot 100$$

End-tidal expiratory CO2 was continuously monitored. Blood pressure was measured before and after each VMR session. VMR was calculated as the percent variation per 1 mm Hg change of end-tidal CO2. After VMR evaluation, the subject completed a visual analogic scale about sleepiness, a visual analogic scale about alertness, and the Stanford Sleepiness Scale.

The following HRV parameters were evaluated for basal recording (basal condition) and during VMR assessment (CO2 condition) by integrating the power density in different frequency intervals: very low frequency (VLF basal, VLF CO2: <0.04 Hz); low frequency (LF basal, LF CO2: 0.04–0.15 Hz); high frequency (HF basal, HF CO2:...
0.15–0.4); and total frequency (TOT\textsubscript{basal}, TOT\textsubscript{CO2} \leq 0.4 Hz). Vagal nerve is the major contributor to the high-frequency component. Although the significance of low-frequency power component is controversial, normalized low-frequency power (LFN=[LF/TOT-VLF]*100) is a reliable measure of sympathetic response to autonomic fibers activation.\(^8\) We estimated the reactivity of LFN (LFN\textsubscript{react}=LFN\textsubscript{CO2}-LFN\textsubscript{basal}) during CO\textsubscript{2} compared with basal condition as a measure of sympathetic responsiveness during VMR assessment.

**tDCS**
A 15-minute 1-mA tDCS was delivered through an active 35-cm\(^2\) sponge electrode positioned over the left M1 (C3 scalp position of the International EEG 10/20 System). The reference was placed above the ipsilateral arm.

**Post-tDCS Evaluation**
Pre-tDCS evaluation procedures were repeated.

**Statistical Analysis**
Stimulation (before vs after tDCS), polarity (A-tDCS vs C-tDCS), and hemisphere (stimulated vs contralateral) effects and their interactions were assessed for basal MFV and VMR (repeated-measures general linear model). The same analysis was applied on behavioral scales and HRV for stimulation*polarity. An effect of VMR evaluation on HRV (CO\textsubscript{2} effect, repeated measures general linear model) was explored.

**Results**
Basal MFV was not different between stimulation, hemisphere, and polarity. No interaction was significant.

A tDCS stimulation*polarity effect (\(P=0.0001\)) on bihemispheric VMR (stimulation*hemisphere; \(P=0.307\)) was found: A-tDCS reduced VMR \(\approx 3.4\% / \text{mm Hg CO}_2\), whereas C-tDCS provided a VMR increase of \(\approx 0.8\% / \text{mm Hg CO}_2\).
tDCS was not found to affect either sleepiness/alertness visual analogic scale or Stanford Sleepiness Scale. Mean heart rate did not show a stimulation*polarity effect. Among HRV parameters, neither single stimulation nor polarity effects were found. LF_{basal}, LF_{CO2}, LFN, LFN_{CO2}, and LFN_{react} showed a stimulation*polarity effect (P<0.031; P<0.008; P=0.032; P<0.001). Mean values analysis demonstrated that LF_{basal} and LFN_{basal} decreased after A-tDCS and increased after C-tDCS. Opposite modifications were found for LF_{CO2}, LFN_{CO2}, and LFN_{react}, thus supporting the hypothesis that tDCS can affect the sympathetic system with polarity specificity (Figure 3A, B). A constant normalized low-frequency reduction from basal to VMR recording was found, even if CO2 effect was not significant for all the conditions (Figure 3B; before A-tDCS, P=0.001; before C-tDCS, P=0.355; after A-tDCS, P=0.427; after C-tDCS, P=0.029). No correlations were found between HRV parameters and VMR changes.

**Figure 3. Transcranial direct current stimulation effect on heart rate variability.**

**A**, Heart rate variability power spectral recordings observed in a paradigmatic subject. Power spectral components of heart rate variability are shown for basal and CO2 condition in a paradigmatic subject. **B**, Normalized low-frequency power and its reactivity (LFN_{react}=LFN_{CO2}-LFN_{basal}) from basal to CO2 condition were also calculated. A stimulation*polarity effect was found to affect LFN_{react} (P<0.001, respectively). LFN, normalized low frequency power.

**Discussion**

The present study demonstrated a polarity-specific effect of tDCS on cerebral VMR in a healthy population. A-tDCS produced a bilateral reduction of VMR, whereas C-tDCS produced its increase.

Cerebral VMR is orchestrated by nervous, myogenic, and metabolic factors. The nervous control is determined mainly through sympathetic efferents regulating arteriolo-capillary caliber. Sympathetic system is not supposed to influence cerebral blood flow under normal conditions, but it plays a key role when the autoregulation limits are overcome. Although a reduction of sympathetic activity lowers the inferior limit, its increase allows maintenance of functional compliance above the superior. Accordingly, an increasing sympathetic activity, as we observed after A-tDCS, could reduce the potential capability of further dilating vessels after a hypercapnic stimulus, as reflected in VMR measurements. The
opposite could be true for a reduced sympathetic tone and C-tDCS effects. Because tDCS effect on cortical excitability is unilateral, its bihemispheric impact on VMR supports the hypothesis of a systemic effect.

An interaction between cortical excitability and the autonomic system is in line with recent findings demonstrating a correlation between the sympathetic activity and M1, and a neuronal connection between the peripheral sympathetic nervous system and M1. Neurophysiological observations also support this assumption.11

TDCS could also affect extracellular pH and [Ca$^{2+}$]; therefore, its influence on the myogenic and the metabolic control of cerebral circulation cannot be excluded. However, these effects might be topographically limited under the electrode, contrasting with bihemispheric effects we observed. Our study has some methodological limitations: autonomic activity was estimated only by HRV and may have been influenced by hypercapnia.

**Conclusion**

In conclusion, tDCS on M1 induced a bilateral modification of cerebral VMR in a polarity-specific manner. Based on consensual changes with HRV, we can speculate that these effects are modulated by the sympathetic nervous system. Further studies are needed to confirm this hypothesis before launching therapeutic trials for stroke with tDCS.

**Disclosures**

None.

**References**


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