Visualization of Local Changes in Vessel Wall Morphology and Plaque Progression in Serial Carotid Artery Magnetic Resonance Imaging

Ronald van ‘t Klooster, PhD; Martine T.B. Truijman, MD; Anouk C. van Dijk, MD; Floris H.B.M. Schreuder, MD; M. Eline Kooi, PhD; Aad van der Lugt, PhD; Rob J. van der Geest, PhD

Carotid atherosclerosis is an important cause of ischemic stroke. Assessment of plaque composition in addition to degree of luminal stenosis can be used to identify patients with increased risk of stroke and assess disease progression. Magnetic resonance imaging (MRI) is an excellent noninvasive imaging technique to assess vessel wall morphology and plaque composition, with good accuracy and reproducibility.1 Serial MRI of the carotid artery is used in several studies which focus on measuring the natural history of carotid artery plaques in symptomatic1 and asymptomatic2 patients and effects of lipid-lowering therapy using statins.3,4 The current standard to analyze serial MRI scans is to compare volume measurements based on manual segmentations of the vessel wall and plaque components. Before comparing the scans, the scans have to be aligned to each other on a slice level. Different approaches exist to align scans from different time points. One study aligns the scans by centering the image stack at each time point over the plaque,1 and another study uses the baseline scan as a reference at the follow-up session to ensure targeting the same arterial segment.4 Alternatively, postprocessing can be used to match the axial images from different time points according to their distance to the carotid bifurcation.2,3 Furthermore, comparison between time points is hindered by inconsistent repositioning of the artery from scan to scan in conjunction with thick image slices. Balu et al5 studied the influence of suboptimal repositioning on measurement precision in serial MRI and identified orientation variability as the most important factor that affected reproducibility. Besides repositioning variability, the current comparison of time points is primarily based on volume measurements, which is a limited representation of the available image data, and no attention is given to local changes or visual presentation of differences between time points.

Therefore, we present a method for analyzing serial MRI scans which uses 3-dimensional (3D) image registration and visualization techniques to enable detailed visual inspection of local differences between time points, providing intuitive insight into the disease progression of an individual patient.

Description of the Innovation

Patient

A 71-year-old man was admitted to the hospital because of loss of strength and sensation of the left arm on awakening. An MRI of the brain revealed several small cortical ischemic lesions in the region of the right middle cerebral artery. Carotid ultrasound showed an ipsilateral carotid artery plaque with ≤30% luminal reduction. A minor stroke of the right hemisphere was diagnosed. The patient was included in a large prospective multicenter study to improve diagnosis of mild to moderate carotid plaques (Plaque At RISK study).6 The institutional Medical Ethical Committee approved the study, and the patient gave written informed consent. The patient was followed up for 2 years, during which he did not experience new ischemic events.

Magnetic Resonance Imaging

Carotid MRI examinations were performed 35 days after the event and after 2 years as previously described.6 The high-resolution multisequence MRI protocol consisted of 5 magnetic resonance sequences: 3D time of flight, 2D T1-weighted (T1w) turbo spin echo, 2D T2w turbo spin echo, 3D inversion recovery–turbo field echo, and postcontrast 2D T1w turbo spin echo. Fifteen transverse adjoining slices of 2 mm each, with an in-plane reconstructed pixel size of 0.3×0.3 mm, covering the entire plaque were acquired.

Image Analysis

The magnetic resonance images at baseline and follow-up were manually segmented by delineating the lumen, outer wall, calcifications, lipid-rich necrotic core (LRNC), and intraplaque
hemorrhage (IPH) according to previously published criteria. Per definition, IPH was always located within the LRNC. Information from all MRI sequences was taken into account during the delineation process. The precontrast T1w images of both time points including segmentations are shown in Figure 1 and demonstrate a slice offset between time points at the bifurcation. The offset was manually corrected by applying a through-plane translation of 1 slice to the follow-up image. To reduce the effect of the high anisotropy of the data on the measurements, the T1w images and segmented vessel wall boundaries were interpolated to a slice thickness of 0.5 mm. The vessel wall boundaries were visually inspected and corrected after interpolation. The interpolated vessel wall boundaries are used in the next section for the calculation of the vessel wall thickness (VWT) and the creation of 3D meshes. The segmentations of the plaque components were not interpolated.

Automated Image Registration
The baseline and follow-up T1w images were aligned to each other using an automated image registration framework which was optimized for carotid artery MRI scans. After registration, point correspondence between the lumen of the baseline and the follow-up image was obtained, that is, for each point on the lumen boundary in the baseline image, the corresponding point on the lumen boundary in the follow-up image is known. Nearest neighbor interpolation was used to extract this information from the manual segmentations.

Visualization Using 3D Surface Meshes
The interpolated lumen and outer wall segmentations were converted into 3D surface meshes. For each point on the lumen mesh, the distance to the nearest point on the outer wall mesh was calculated resulting in a local VWT measure. The VWT is color coded on the lumen mesh to provide a 3D visualization. The VWT analysis was repeated for the follow-up segmentation.

By using the point correspondence between the baseline and follow-up lumen, differences in measurements between baseline and follow-up can be visualized by color coding this difference on the baseline luminal surface mesh. Similarly, increase or decrease of plaque components can be visualized by color coding the lumen surface. Presence of a plaque component was indicated on a lumen mesh point when a plaque component was present between that lumen mesh point and its closest point on the outer vessel wall. Nearest neighbor interpolation was used to extract this information from the manual segmentations.

Results of Pilot Testing
First, volume- and area-based comparison between baseline and follow-up was performed. Lumen volume at baseline was 1.525 and 1.507 mL at follow-up, vessel wall volume was 1.634 versus 1.577 mL, calcification volume was 0.017 versus 0.015 mL, and LRNC was 0.378 versus 0.444 mL. The external carotid artery was excluded from the volume- and area-based measurements. Figure 2 shows the slice-based area measurements of the lumen, outer vessel wall, calcifications, and LRNC of the manually aligned baseline and follow-up slices. The volume and area measurements demonstrate a mixed result; a consistent increase in LRNC was observed, whereas the other components showed a small decrease and little variation between baseline and follow-up.

Figure 3 shows the 3D visualization of VWT at baseline and follow-up, change in VWT, and progression or regression of LRNC with or without IPH over time. All metrics are color coded on the lumen surface, and appropriate color maps are chosen. A bipolar color map was chosen for Figure 3C in which gray corresponds to no change, blue to a decrease, and red to an increase in VWT. The strong red regions indicate a clear increase in VWT.
The absence of strong blue regions suggests accurate registration between baseline and follow-up. The increase in VWT is positively correlated with the presence of LRNC (Figure 3D). The 3D visualizations are interactive which allows the clinician to explore the results using zoom and rotation.

The change in VWT was quantified for locations inside the vessel wall which were thickened (VWT >1 mm) and grouped into locations without and with LRNC (with or without IPH; Figure 4). The mean change and SD in VWT was −0.02±0.41 mm for thickened vessel wall and 0.36±0.52 mm for the LRNC locations. Wilcoxon rank-sum test demonstrated a significant difference between both groups (P<0.001).

Conclusions
We introduced a new method to analyze and present serial MRI data of the carotid artery vessel wall. Three-dimensional image registration is used to obtain point correspondence between images from different time points, which enables assessment of local changes in plaque morphology. Three-dimensional visualization techniques are applied to present changes in vessel wall morphology using difference maps which are color coded on a mesh of the lumen segmentation of the baseline image and related to the presence of different atherosclerotic plaque components in the vessel wall. The bipolar color map of the difference map as shown in Figure 3C allows the clinician to differentiate between small and substantial changes in VWT between time points. Moreover, the presented tool can be used to demonstrate a significant increase in VWT over time for locations with LRNC with or without IPH.

Both observations could not be deducted from the traditional volume or area measurements.

The 3D visualizations provide an interactive and intuitive way to represent measurements extracted from the original image data. The visualizations as presented in this work provide insight in the change in VWT and progression or regression of different plaque components. Other measurements, for example, changes in degree of stenosis, can be visualized using a similar methodology. These new visual data analysis tools provide clinicians with a detailed view of atherosclerotic disease progression of individual patients and can potentially improve understanding of the effect of changes in plaque components on local plaque progression/regression. Compared with conventional slice-wise comparison, which can only partly account for interscan misalignment, the presented approach based on 3D registration may potentially have a positive impact on measurement reproducibility. Further research on a larger cohort of patients and multiple readers is warranted to investigate this aspect.

To conclude, the presented method to analyze and visualize changes over time for carotid artery MRI is an improvement over the traditional volume-based analysis as it provides a detailed view of local differences between baseline and follow-up scans and increased insight into the disease progression of an individual patient.

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Disclosures
Dr van der Lugt receives a research grant from GE Healthcare for testing magnetic resonance sequences for plaque imaging. The other authors report no conflicts.

References


**Key Words:** atherosclerosis ▪ carotid arteries ▪ computer-assisted follow-up studies ▪ computer-assisted image interpretation ▪ image processing ▪ magnetic resonance imaging ▪ stroke
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表5. FDA,HC和EMA药物标签中的药物相互作用比较

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注：*指未知/无数据

临床和研究创新

颈动脉磁共振成像中血管壁局部形态和斑块进展的可视化成像

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Stroke. 2014;45:e160-e163. 第三军医大学附属新桥医院神经内科 卫飞 译；帅杰 校

颈动脉磁共振成像是脑血管病中的重要成像技术，评估颈动脉变窄以及和颈动脉粥样斑块有关的临床风险。本研究旨在研究颈动脉磁共振成像（MRA）在评估颈动脉粥样斑块的自然病程、患者特定因素以及非侵入性成像技术在评估颈动脉粥样斑块的形态和成分方面的性能。

目的：评估颈动脉粥样斑块的自然病程。

方法：使用磁共振血管造影（MRA）对颈动脉粥样斑块进行随访。研究对象为2014年8月的18个病例，包括9个男性和9个女性。所有患者均接受MRA随访。

结果：在8个月的随访期内，所有患者均未发生新的颈动脉事件。

结论：颈动脉磁共振成像可以评估颈动脉粥样斑块的自然病程。
初步实验结果

首先，完成了基线和随访图像间基于体积和面积的比较。基线管腔体积是1.525ml，而随访图像体积是1.507ml，管壁体积分别是1.634ml和1.577ml，钙化体积分别是0.017ml和0.015ml，而LRNC是0.378ml和0.444ml。颈外动脉未做基于体积和面积的测量。图2示手工对齐基线和随访层面后，基于层面管腔、外壁、钙化、LRNC面积测量值比较结果。体积和面积测量结果是一个混杂的结果；在基线和随访图像中，LRNC可见一致增加，而其它成分少量减少或没有变化。图3示基线和随访图像中VWT的3D图像，VMT的变化，以及全程包含不含IPH的LRNC的进展或逆转。所有病损在管腔表面线性编码，从而显示明显的面貌。图3C示对齐后图像，灰色代表VWT无变化，红色代表减少，蓝色代表增加。图3D示对齐后图像，灰色代表VWT无变化，红色代表减少，蓝色代表增加。图3A和B示三维表面格点矩阵分别显示基线、随访期局部血管壁厚度(VWT)(A和B)，一段时问后的血管壁厚度差异(C)和一段时间后伴或不伴斑块内出血的富脂坏死核心(LRNC)进展或逆转(D)。

VWT的变化可定量成增厚的血管壁内(VWT>1mm)的位置变化，分成无LRNC和有LRNC(有或没有IPH)两组(图4)。VWT变化的均值和标准差为-0.02±0.41mm(单纯血管壁增厚组)和0.36±0.52mm(有LRNC组)。Wilcoxon秩和检验示两组间有显著意义(P<0.001)。

结论

我们引入一个新方法分析和展示颈动脉血管壁的系列MRI数据。三维图像配准用于不同时间点获取图像的层面对应关系，使得评估斑块形态的局部变化成为可能。3D显像技术用不同的彩色图展示血管壁形态的变化，用颜色编码基线图像中管腔表面的热点阵列，对血管壁不同动脉斑块硬化斑块的存在和与VMT的变化，以及全程包含不含IPH的LRNC的进展或逆转。所有病损在管腔表面线性编码，从而显示明显的面貌。图3C示对齐后图像，灰色代表VWT无变化，红色代表减少，蓝色代表增加。图3D示对齐后图像，灰色代表VWT无变化，红色代表减少，蓝色代表增加。图3A和B示三维表面格点矩阵分别显示基线、随访期局部血管壁厚度(VWT)(A和B)，一段时问后的血管壁厚度差异(C)和一段时间后伴或不伴斑块内出血的富脂坏死核心(LRNC)进展或逆转(D)。

图2通过手工对齐基线和2年随访时的扫描图像，可看到差异显著的血管壁厚度变化。图3A示基线图像中管腔表面的血管壁厚度变化，图3B示随访图像中管腔表面的血管壁厚度变化，图3C和D示对齐后图像，灰色代表VWT无变化，红色代表减少，蓝色代表增加。图3C示对齐后图像，灰色代表VWT无变化，红色代表减少，蓝色代表增加。图3A和B示三维表面格点矩阵分别显示基线、随访期局部血管壁厚度(VWT)(A和B)，一段时问后的血管壁厚度差异(C)和一段时间后伴或不伴斑块内出血的富脂坏死核心(LRNC)进展或逆转(D)。

参考文献