Safety, Feasibility, and Efficacy of Vagus Nerve Stimulation Paired With Upper-Limb Rehabilitation After Ischemic Stroke

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Background and Purpose—Recent animal studies demonstrate that vagus nerve stimulation (VNS) paired with movement induces movement-specific plasticity in motor cortex and improves forelimb function after stroke. We conducted a randomized controlled clinical pilot study of VNS paired with rehabilitation on upper-limb function after ischemic stroke.

Methods—Twenty-one participants with ischemic stroke >6 months before and moderate to severe upper-limb impairment were randomized to VNS plus rehabilitation or rehabilitation alone. Rehabilitation consisted of three 2-hour sessions per week for 6 weeks, each involving >400 movement trials. In the VNS group, movements were paired with 0.5-second VNS. The primary objective was to assess safety and feasibility. Secondary end points included change in upper-limb measures (including the Fugl–Meyer Assessment-Upper Extremity).

Results—Nine participants were randomized to VNS plus rehabilitation and 11 to rehabilitation alone. There were no serious adverse device effects. One patient had transient vocal cord palsy and dysphagia after implantation. Five had minor adverse device effects including nausea and taste disturbance on the evening of therapy. In the intention-to-treat analysis, the change in Fugl–Meyer Assessment-Upper Extremity scores was not significantly different (between-group difference, 5.7 points; 95% confidence interval, −0.4 to 11.8). In the per-protocol analysis, there was a significant difference in change in Fugl–Meyer Assessment-Upper Extremity score (between-group difference, 6.5 points; 95% confidence interval, 0.4 to 12.6).

Conclusions—This study suggests that VNS paired with rehabilitation is feasible and has not raised safety concerns. Additional studies of VNS in adults with chronic stroke will now be performed.

Clinical Trial Registration—URL: https://www.clinicaltrials.gov. Unique identifier: NCT01669161.

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Key Words: deglutition disorders • intention to treat analysis • rehabilitation • stroke • vagus nerve
neuroplasticity to promote reorganization of neural networks is required to more fully recover motor function.3 However, no practical and effective method exists to achieve this and even if such changes occur, it is unclear whether they are clinically meaningful or long term. This study is a preliminary investigation of an intervention designed to promote specific neuroplasticity; vagus nerve stimulation (VNS) paired with movement to drive task-specific plasticity in the motor cortex.10–12 VNS activates neurons in the basal forebrain and locus coeruleus and results in release of acetylcholine and norepinephrine, respectively, which are known to facilitate reorganization of cortical networks.13 We recently demonstrated in a rat model of ischemic stroke that pairing forelimb rehabilitation with VNS significantly increases recovery of forelimb speed and strength when compared with rehabilitation alone.14,15 Our subsequent studies demonstrated that VNS paired with rehabilitative training also improves recovery in a rat model of intracerebral hemorrhage,16 and that precise timing of VNS with specific motor movements yields optimal recovery.17

We hypothesize that VNS paired with upper-limb rehabilitation will result in greater recovery of arm function than rehabilitation alone in adults with chronic ischemic stroke. We performed the first-in-human evaluation of VNS paired with upper-limb rehabilitation after ischemic stroke. The main objective of the study was to evaluate the safety and feasibility of paired VNS therapy after stroke and to provide clinical data for sample size calculations for larger studies.

Methods

Study Design and Participants

We performed a randomized open active comparator study with blind-ed objective end point assessment. We compared VNS paired with rehabilitation with rehabilitation alone in subjects with arm weakness because of chronic ischemic stroke. Participants were enrolled at 2 stroke centers in the United Kingdom (NHS Greater Glasgow and Clyde and Newcastle upon Tyne NHS Foundation Trust). Study approval was granted by the Medicine and Healthcare Regulatory Authority and by the West of Scotland Research Ethics Committee. Participants provided voluntary, written informed consent. The trial was registered on clinicaltrials.gov (NCT01669161) and the protocol is at http://www.microtransponder.com/?page_id=972.

Patients with a history of unilateral supratentorial ischemic stroke that occurred at least 6 months before, aged ≥18 years and ≤80 years, with an Action Research Arm Test (ARAT) score of 15 to 50 (inclusive, indication moderate to severe arm impairment) were eligible for inclusion. Full inclusion and exclusion criteria are given in the Methods in the online-only Data Supplement.

Study Visits and Data Collection

Baseline Assessments

Participants had 3 visits before starting rehabilitation therapy. The first was performed soon after consent was obtained to confirm eligibility. A second was performed at least 2 weeks later at which point randomization and structural brain magnetic resonance imaging (MRI) were performed. Device implantation was then scheduled in participants randomized to the VNS group. A third baseline assessment was performed after device implantation (or before the start of rehabilitation in rehabilitation-only participants). Each assessment included a detailed medical history and details of the index stroke, assessment of eligibility, and measures of arm function. The measures of arm function used were the upper extremity Fugl–Meyer assessment (FMA-UE),18 ARAT,19 grip and pinch strength (via a hand-held dynamometer),20 Box and Block test,21 9-hole peg test,22 and robotic assessment using an InMotion Technologies robot.23 We also used the Stroke Impact Scale.24

All observers received training in these measures before performing any assessments. This included written materials, practice at an investigators meeting, and (for the FMA-UE and ARAT score) review and scoring of recorded assessments followed by discussion to agree and confirm understanding of scoring rules.

Randomization and Masking

Enrolled participants were randomized, via an interactive voice response system (Robertson Center for Biostatistics, University of Glasgow), to receive VNS plus rehabilitation or rehabilitation alone. Randomization was stratified by site, and block size was variable. Because of the nature of surgical device implantation, investigators, therapists, and participants were not blinded to treatment allocation. We attempted to ensure that outcome assessors were blinded by using assessors not involved in other aspects of the trial, by asking participants not to discuss their treatment allocation and to cover the chest and neck. We asked assessors to confirm that they were blinded before outcomes assessments.

Magnetic Resonance Imaging

MRI data were acquired on 3T MRI scanners. Full details are given in the Methods in the online-only Data Supplement. The extent of injury to the corticospinal tract (CST) was quantified as previously described.23 We defined injury to the CST by the CST fractional anisotropy ratio and mean diffusivity ratio between the stroke and the nonstroke side and the volume of the stroke lesion within the CST.

VNS Device Implantation

Implantation was performed after the second baseline assessment in the VNS and rehabilitation group. Participants had a preoperative assessment, which included anesthetic review and fiber optic laryngoscopy (Figures I–VII in the online-only Data Supplement). Participants were typically admitted on the morning of device insertion and were discharged within 24 hours. Device implantation was performed under general anesthesia by either a Consultant Ear Nose and Throat surgeon (Glasgow) or a Consultant Neurosurgeon (Newcastle). The implantation involved placement of the stimulation electrodes of the leads (Model 304; Cyberonics Inc., Houston, TX) on the left vagus nerve in the left carotid sheath. The lead is then tunnelled subcutaneously to a subcutaneous pocket created in the left pectoral region where it is attached the implantable Vivistim pulse generator. Full details are available in the Methods in the online-only Data Supplement.

Rehabilitation Training

All participants received a 6-week course of 2-hour therapy sessions 3x per week. All sessions started with 10 to 15 minutes of stretching exercises (without VNS). Thereafter, 7 standardized tasks were performed (Methods in the online-only Data Supplement). Tasks included reach and grasp, handle turning, gross movement, object flipping, simulated eating tasks, inserting objects, opening bottles, and additional tasks selected by participants as priorities for improvement. Subjects performed at least 300 to 400 movements in each session that were modified or progressed to be achievable, but challenging. Each subject spent ≥10 minutes on each of the 7 tasks per during each session. All tasks were delivered by a licensed stroke physiotherapist. Therapy sessions were video recorded to monitor the treatment delivered.

VNS Protocol

A wireless control interface was used to communicate with the VNS device and deliver stimulation during therapy sessions. A laptop
with the Stroke Application Programming Software was used to program the IPG and initiate VNS. The stimulation was manually triggered by the therapist using a push button, while the patient performed a task (Figure 1). Stroke Application Programming Software allows the therapist to control the relative timing of stimulation to therapy exercises using the push button. The software also allows the physician to control the stimulation parameters (amplitude [mA], frequency [Hz], pulse width [μs], and duration [ms]), captures patient programming history, and checks lead impedance and battery status. A 500-ms burst of VNS was delivered to the VNS group during each movement (the rehabilitation-only group did not have a device implanted). Each simulation consisted of fifteen 0.8-mA, constant current, charge balanced pulses (100-μs pulse width, 30-Hz frequency). These stimulation parameters grew out of hypothesis-driven research in humans and animal models, including studies of cortical map plasticity and electroencephalogram desynchronization using VNS. Note stimulation was only delivered to the left vagus nerve to avoid activation of the sinoatrial node (which is innervated by the right vagus nerve), but bilateral neuronal connections mean stimulation should affect both cerebral hemispheres. Full details are given in the Methods in the online-only Data Supplement.

Outcome Assessments
These were performed on days 1, 7, and 30 after the conclusion of rehabilitation therapy in both groups. The FMA-UE, ARAT, grip, and pinch strength via a hand-held dynamometer, Stroke Impact Scale, Box and Block test, and 9-hole peg test were assessed. The ARAT, grip strength, Box and Block tests, and 9-hole peg test were also measured at the end of the second and fourth week of the 6-week therapy period. Assessments were always performed in the same order, with a break halfway through the visit to complete questionnaires. Long-term follow-up and postimplantation care is described in the Methods in the online-only Data Supplement.

Statistical Analysis and Study End Points
Because this was a pilot study, no formal sample size calculation was performed. An intention-to-treat and per-protocol analysis were performed. The per-protocol analysis included participants who had at least 12 of the 18 therapy sessions and who were not taking any drugs that may interfere with VNS during the study. The numbers of serious and nonserious adverse events (AEs) are described, along with the numbers who completed the therapy protocol.

The main study safety end point was the number of serious AEs related to therapy, and the main feasibility end point was the number of participants who completed therapy protocol. The main efficacy assessment was change in FMA-UE score between the main baseline assessment and the first post-therapy visit. Secondary end points were changes in ARAT, Box and Block, 9-hole peg test, and grip strength. We also assessed whether participants improved by the minimum clinically significant difference in the FMA-UE and ARAT scores. This was defined as 26 points in the FMA-UE score and ≥25 points in the ARAT score. The efficacy end points for change in value were compared using ANCOVA with adjustment for the baseline value. To compare the percentage of improvers in each group, we used Fisher exact test. Finally, we explored the levels of the baseline MRI measures in relation to clinical response within each group using 2-sample t tests and Pearson correlations.

Results

Study Participants
Seventy-one patients were screened, of whom 21 were enrolled between February 2013 and April 2014 (16 at the Glasgow site and 5 at the Newcastle site). Twenty participants were randomized (1 withdrew because of improvement in arm function during the baseline assessment phase and no longer wished to continue). Nine participants were randomized to VNS and rehabilitation and 11 to rehabilitation only. One patient in the VNS group received medication that may interfere with VNS so was excluded from the per-protocol analysis. A consort diagram is shown in Figure 2.

All participants were white and could ambulate independently. Baseline characteristics are shown in Table 1. Groups seemed balanced for time from stroke, age, sex, handedness, and baseline ARAT, but there was a 5-point difference in the baseline FMA-UE scores (lower in the VNS group).
Feasibility
All randomized participants attended all planned therapy sessions. In the VNS group, the average duration of therapy (excluding stretching) was 72 minutes (SD, 8; range 38–90 minutes). This compared with 79 minutes (SD, 8; range 53–113 minutes) in the rehabilitation-only group. Participants performed an average of 414 movements paired with VNS during a session in the VNS group (SD, 124; range, 104–796). This compared with 463 movements (SD, 157; range, 165–876) in the rehabilitation-only group. One participant, who had a good clinical response, opted for device removal at the end of the study. All remaining participants have the device in situ and are undergoing longer-term follow-up.

Safety
There were 22 AEs in the 8 participants in the VNS group (11 of which were adverse device effects in 5 participants) when compared with 10 AEs in 3 participants in the rehabilitation-only group. Two participants had a serious AE in the VNS group, none of which were serious device effects. One participant had 4 serious AEs in the rehabilitation group. No AEs were related to the rehabilitation therapy itself. The serious AEs are summarized in Table 2.

The adverse device effects were minor with the exception of one (moderate severity) and all resolved. This participant had a left vocal cord palsy and dysphagia after device implantation. Dysphagia settled over a 3-week period. This was successfully managed as an outpatient. VNS was stopped after 2 weeks in case it would hinder recovery; however, the participant continued to receive rehabilitation only. To exclude an underlying diagnosis for vocal cord palsy (the patient was an ex-smoker), computed tomographic scan of the neck and thorax was performed. This excluded any other cause but revealed left-sided phrenic nerve palsy, and the participant remained under active follow-up to exclude other causes. This vocal cord and phrenic nerve palsy had resolved at 9-month follow-up. One participant reported nausea after a single long session of VNS and rehabilitation. One participant reported a taste disturbance after surgery (metallic taste) that continued during the first 2 weeks of therapy. One participant reported mild dysphagia in the evening after therapy sessions (manifest as finding it more difficult to swallow a capsule that evening only). None of these minor symptoms required changes to the therapy protocol, and all resolved on the day of the therapy session. Six participants had a slight hoarseness or neck tingling during stimulation, 3 were not aware of stimulation.

Efficacy
The mean change in FMA-UE scores in the VNS group was +8.7 (5.8) versus +3.0 (6.1) in the rehabilitation-only group (between-group difference, 5.7 points; 95% CI, −0.4 to 11.8; P=0.064; Figure 3). In the per-protocol analysis (n=19), the mean change in FMA-UE score was +9.6 points (5.3) and +3.0 points (6.1) in the rehabilitation-only group (between-group difference, 6.5 points; 95% CI, 0.4 to 12.6; P=0.038). Six (66.7%) achieved a clinically meaningful response on the FMA-UE score in the VNS group compared with 4 (36.4%) in the rehabilitation-only group (P=0.17). There were no significant differences in the other secondary efficacy end points (Table 3) including robotic kinematic measures (data not shown).

Response in Relation to MRI Measures
There were no significant differences in MRI measures at baseline between groups although there was a trend for baseline infarct volume, CST overlap volume, and mean diffusivity ratio to be higher and for fractional anisotropy ratio to be lower in VNS participants (Table I in the online-only Data Supplement).
There was no significant correlation between baseline MRI variables and change in UEFM score (Table II in the online-only Data Supplement) in either group. However, infarct volume, CST overlap volume, fractional anisotropy ratio, and mean diffusivity ratio were significantly worse at baseline (P<0.05) in VNS responders compared with rehabilitation-only responders (Table III in the online-only Data Supplement).

Discussion
This trial provides initial evidence of safety and feasibility of a novel neurostimulation technique, which in conjunction with rehabilitation for the upper limb, aims to promote neuroplasticity specific to improved upper-limb function. The data provide no signal of harm. Our study was not designed to test clinical efficacy, and our findings are preliminary. However, the per-protocol analysis demonstrated a significantly greater improvement in FMA-UE scores in VNS-treated participants than in controls. Baseline MRI data showed a significant difference in baseline MRI variables between responders in the VNS group and responders in the rehabilitation-only group. Whether this means VNS therapy allows recovery to occur in some participants who would not respond to conventional rehabilitation techniques requires rigorous testing in further randomized clinical trials.

Our innovation is to use short bursts of VNS paired with specific movements to restore lost motor skills. To the best of our knowledge, this is an entirely novel use of VNS. This method of VNS is sharply distinct from the current clinical use of VNS for the treatment of refractory epilepsy and depression, where VNS is delivered on 30 seconds and on 5 minutes off cycle. The stimulation used in the current study delivered <1% of the charge delivered with the Food and Drug Administration–approved protocols for epilepsy and depression. VNS paired with rehabilitation has been shown to improve recovery of forelimb function in several models of experimental stroke. VNS has also shown promise in a small study of participants (n=10) with severe chronic tinnitus, a disorder of abnormal central auditory system plasticity although this was an open study and confirmatory data are needed. We have based our stimulation parameters on both animal and human data. We have recently found (in rat models) that pairing tones with 0.4 or 0.8 mA is sufficient to reorganize auditory cortex, whereas pairing tones with 1.2 or 1.6 mA do not result in detectable cortical plasticity.

This observation closely mimics previous studies in epilepsy patients where moderate but not high VNS current was memory enhancing. However, further clinical studies will be needed to define the optimum stimulation parameters for the stroke indication.

The mechanisms by which paired VNS exerts its effects on cortical neurons are not completely understood. However, it is well known that nucleus basalis and locus coeruleus neurons are activated during VNS via activation of nucleus tractus solitarius. When stimulated, these neurons release acetylcholine and norepinephrine throughout the cortex. It is important to note that even though acetylcholine and norepinephrine are released throughout cortex, cortical plasticity is specific to the set of neurons driven by the stimulus (eg, sound or movement). Both behavioral and neurophysiologic changes can be observed when nucleus basalis or the vagus nerve is directly stimulated in short bursts and paired with sound or a movement. Short-term stimulation of locus coeruleus neurons before training also seems to enhance learning and memory. Thus, a reasonable mechanistic explanation exists for why pairing VNS with sensory or motor events could be an effective therapeutic approach for enhancing specific neuroplastic change.

Tolerability of surgery and stimulation was similar in our cohort when compared with that seen in current clinical applications although numbers were small. One patient developed a vocal cord palsy after device implantation. Overall, we conclude that there were no significant safety concerns that would preclude further study. This does not suggest that there are no important considerations for participants considering participation in future trials, or for patients should this treatment be introduced to clinical practice. On the basis of extensive experience of VNS in patients with epilepsy, we expect to see infection related to device implantation in ≈1% of participants, and other complications associated with anesthesia and surgery could arise. We minimized these risks by prescribing perioperative low molecular weight heparin in place of oral anticoagulants or by substituting aspirin for clopidogrel where appropriate. Some VNS devices are MRI compatible, but we excluded patients who had a condition requiring MRI surveillance and patients who would not be able to undergo contrast-based computed tomographic imaging.

Although each therapy session in the trial was participant and goal specific, the duration and intensity of therapy were...
higher in the rehabilitation-only group so is unlikely to have confounded the results. The improvement in function seen in the control group was similar to that demonstrated in previous clinical trials of intensive upper-limb therapy including robotic therapy and constraint induced movement therapy. However, it should be noted that participants recruited to trials of treatments such as robotic therapy had stroke symptoms that were typically more severe than those included in our study.

When interpreting the results of functional recovery from a mechanistic stand point, there is often the question of recovery of actual function versus compensation. To our knowledge, there is no measure that distinguishes the difference between compensatory and restorative change. Subtle compensatory strategies, such as accessory trunk motion, are controlled for with the choice of the Fugl–Meyer assessment tool. The nature of the Fugl–Meyer test is to measure motor impairment in stroke and because of the assessment of isolated movement of body parts, thus, typical clinical compensatory strategies are well controlled for. We found significant differences between responders in the VNS group and rehabilitation-only group. Infarct volume and measures of CST involvement were worse in VNS responders when compared with control responders. The CST fractional anisotropy ratio is known to be a predictor of long-term motor impairment and was lower in VNS responders. We hypothesize that VNS may be able to generate clinical responses in patients who would otherwise not respond to standard treatments through enhancing neuroplasticity.

There are several strengths to this study. The study was randomized reducing the risk of selection bias. Blinded assessors not involved in the day-to-day treatment of participants assigned outcomes. We had 98% follow-up, and all participants completed the therapy protocol. The control group received intense rehabilitation similar to the VNS group, rather than typical standard of care.

Table 3. Efficacy Measures

<table>
<thead>
<tr>
<th>Measure</th>
<th>Difference Between Groups ITT</th>
<th>P Value</th>
<th>Difference Between Groups PP</th>
<th>P Value</th>
</tr>
</thead>
<tbody>
<tr>
<td>FMA-UE</td>
<td>5.71 (−0.36 to 11.79)</td>
<td>0.064</td>
<td>6.50 (0.42 to 12.58)</td>
<td>0.038</td>
</tr>
<tr>
<td>ARAT</td>
<td>0.41 (−3.98 to 4.80)</td>
<td>0.845</td>
<td>0.92 (−3.64 to 5.49)</td>
<td>0.674</td>
</tr>
<tr>
<td>Grip strength</td>
<td>−2.63 (−6.42 to 1.17)</td>
<td>0.162</td>
<td>−2.69 (−6.57 to 1.37)</td>
<td>0.180</td>
</tr>
<tr>
<td>NHPT</td>
<td>43.91 (−28.10 to 115.92)</td>
<td>0.201</td>
<td>43.91 (−28.10 to 115.92)</td>
<td>0.201</td>
</tr>
<tr>
<td>Box and Block test</td>
<td>−0.47 (−6.02 to 5.09)</td>
<td>0.861</td>
<td>−0.3 (−6.06 to 5.47)</td>
<td>0.914</td>
</tr>
</tbody>
</table>

The difference between groups and 95% confidence interval is shown. Positive values represent greater change in VNS-treated participants for all measures except the NHPT. Only participants who could complete the NHPT were included in the NHPT analysis. Data are shown for the ITT analysis (n=9 VNS and n=11 rehabilitation-only participants for all assessments [except NHPT where n=5 and n=7, respectively]) and for the PP analysis (n=8 VNS and n=11 rehabilitation-only participants [except NHPT where n=5 and n=7, respectively]). ARAT indicates Action research arm test; FMA-UE, Fugl–Meyer assessment, upper extremity; ITT, intention to treat; NHPT, 9-hole peg test; PP, per protocol; and VNS, vagus nerve stimulation.
There are limitations to consider. This study was not blinded to either the physiotherapist delivering the therapy or the participant, and there was no sham stimulation group. Although we asked participants not to discuss their treatment allocation during outcomes assessments, we cannot exclude that assessors picked up on visual cues such as a scar in the neck from lead insertion. Furthermore, the study was small leading to imprecision in some of the efficacy assessments.

In conclusion, VNS paired with rehabilitation therapy is feasible in adults with arm weakness ≥6 months after ischemic stroke. It also seems to be acceptably safe for further study.

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Disclosures
Dr Dawson has received reimbursement for conference attendance and travel expenses and was a co-investigator of the Stroke2000 study. His work has been supported by the National Institute for Health Care and Clinical Excellence; 2013. Dr Dawson has received reimbursement for conference attendance and travel expenses and was a co-investigator of the Stroke2000 study. His work has been supported by the National Institute for Health Care and Clinical Excellence; 2013.

References


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SUPPLEMENTAL MATERIAL

Safety, Feasibility and Efficacy of Vagus Nerve Stimulation Paired with Upper Limb Rehabilitation Following Ischemic Stroke
Supplementary Methods

Complete List of Inclusion Criteria:

1. History of unilateral supratentorial ischemic stroke that occurred at least 6 months prior
2. Age >18 years and <80 years
3. Right or left sided weakness of upper extremity
4. ARAT score of 15 to 50 (inclusive of 15 and 50)
5. At least 5 degrees of active wrist extension
6. Modified Rankin Score of 2, 3, or 4

Note patients above the age of 80 years were excluded from this first study for safety reasons and as we recognise patients above the age of 80 years have more variable outcome and may respond differently to stroke treatments.

Complete List of Exclusion Criteria:

1. Hemorrhagic stroke
2. Any deficits in language or attention that interferes with reasonable study participation
3. Presence of significant apraxia
4. Profound sensory loss
5. Active major neurological or psychiatric diagnosis that would likely interfere with study protocol including alcohol or drug abuse
6. Patient receiving any therapy (medication or otherwise) at study entry that would interfere with VNS (e.g. drugs that interfere with neurotransmitter mechanisms – such
as anticholinergics, adrenergic blockers, etc.). Additionally, no psychoactive medications – including nicotine – may be used during the acute study. *

7. Prior injury to vagus nerve (e.g., injury during carotid endarterectomy)

8. Severe depression (Beck Depression Scale ≥ 29)

9. Not considered candidate for a device implant surgery (history of adverse reactions to anaesthetics, poor surgical candidate in surgeon’s opinion, etc.)

10. Any other implanted device such as a pacemaker or other neurostimulator; any other investigational device or drug

11. Medical or mental instability (diagnosis of personality disorder, psychosis, or substance abuse)

12. Pregnant or plan on becoming pregnant or breastfeeding during the study period

13. Currently require, or likely to require, diathermy during the study duration

14. Any health problem requiring surveillance with MRI imaging

15. Active rehabilitation within 4-weeks prior to therapy

16. Botox injections or any other non-study active rehabilitation of the upper extremity 4-weeks prior to and during therapy

17. Severe spasticity (Modified Ashworth ≥ 3)

*Excluded drug classes included muscarinic antagonists, norepinephrine re-uptake inhibitors, centrally acting beta-blockers, benzodiazepines, selective serotonin re-uptake inhibitors, nicotinic antagonists, centrally active alpha-blockers, tricyclic anti-depressants, anti-psychotic drugs, anti-epileptic drugs.

**MRI Imaging and Data Analysis**
MRI data was acquired on a Siemens Verio 3T MRI scanner (Erlangen, Germany) in Glasgow and on a Philips Intera Achieva 3T MRI scanner (Eindhoven, Netherlands) in Newcastle. The MRI protocol included 3D T1-weighted, T2-weighted fluid suppressed and susceptibility weighted imaging sequences. Diffusion Tensor Imaging (DTI) data was also acquired with a b-value of 1000s.m⁻² and 21 diffusion directions (Glasgow) and a b-value of 800s.m⁻² and 16 diffusion directions (Newcastle). Infarct volume was measured and corticospinal tract (CST) integrity was assessed using the fluid suppressed T2-weighted imaging data and the DTI respectively. We defined injury to the corticospinal tract by the CST fractional anisotropy (FA) ratio and mean diffusivity (MD) ratio between the stroke and non-stroke side, the mean diffusivity ratio and the volume of the stroke lesion within the CST.

**Device implantation**

In this study, a single Otolaryngologist, Head and Neck Surgeon with an interest in vagus nerve stimulation performed device implantation at the Glasgow site and a single Neurosurgeon performed implantation at the Newcastle site. Detailed operative procedures from the Glasgow site are included for reference. Normal vocal cord movement was confirmed by flexible laryngoscopy prior to procedure. The procedure was performed under general anaesthesia. The subject was positioned on the operating table in the supine position with their neck extended through use of a shoulder roll, with the head supported on a head ring. The skin was prepared using surgical antiseptic solution and the operative area was square draped. A horizontal neck crease incision was created left of the midline over the anterior edge of the sternocleido-mastoid (SCM) muscle at level of the cricoid cartilage. The left vagus nerve was chosen as it has fewer cardiac efferent fibres going to the sino-atrial node,
thus minimising risk of arrhythmias. The level of cricoid was chosen for incision to allow dissection of an adequate length of nerve for placement of the probes without encountering significant branches. The platysma muscle was divided and sub platysmal flaps are raised. The anterior border of the SCM was identified and lateralised. Omohyoid was divided and the carotid sheath was dissected to expose the vagus nerve. The vagus nerve was identified and confirmation of an intact functional nerve was confirmed with a monitoring probe. A section of the vagus nerve was cleared of fascia. (Supplementary figure I)

The helical nerve stimulation leads (Model 304, Cyberonics Inc., Houston, TX) was then coiled around the nerve. (Supplementary figure II)

Adequate contact of both leads with the nerve was confirmed by application of the Neural Integrity Monitor (Medtronic) probe to the end of the stimulator wire at two
positions. Each position correlated with a single vagus nerve stimulator lead.

(Supplementary figure III)

Teflon cuffs were placed around the wire and sutured to soft tissue within the neck thereby securing it in place with a release loop to allow neck movement without tension being applied to the nerve which could cause lead displacement.

(Supplementary figure IV)

A subcutaneous pocket was then created in the left pectoral region and the wire was tunnelled to allow the wire to connect to the pulse generator (Model 1000 Vivistim System, MicroTransponder Inc., Austin, TX). Contact of the leads was re-checked with the NIM probe to prior to securing the wire to the pulse generator. The pulse generator was placed within the subcutaneous pocket and sutured in place.

(Supplementary figure V)
Activity of the pulse generator was calibrated by a wireless programming device connected to computer running proprietary software (MicroTransponder) and impedance was measured across the leads. Integrity of the circuit was confirmed by observing corresponding nerve activity on NIM monitor when a stimulation pulse is triggered by the wireless device. (Supplementary figure VI).

The omohyoid was repaired and the neck and chest incisions closed. Participants were either discharged later that day or on the following day.

**Details of Stimulation Parameters and SAPS Software**

The Vivistim® system is an active implantable device consisting of an IPG, an implantable lead, external controller wand (for communication) and custom programming software. A netbook computer is loaded with the Stroke Application Programming Software (SAPS) and is used to set the stimulation parameters and load them into the patient’s IPG via the wand. SAPS is a custom software used to program the stimulation parameters and imitate VNS via a pushbutton.
During therapy the IPG was programmed to output a 0.5 second burst of stimulation. The stimulation consisted of a 30 Hz signal of 100 µsecond constant current pulses with an amplitude of 0.8 mA.

**Therapy Tasks**

The therapy tasks consisted of the following:

1. Reach and grasp objects

The task involves the ability to reach, grasp, manipulate and release a variety of objects along with a variety of strength and range of motion requirements and some degree of endurance (i.e., being able to stand during task performance).

2. Turning doorknobs and turning keys

The patient reaches and manipulates a variety of styles of doorknobs and latches. The patient also must insert and turn a key in a variety of locks.

3. Gross Movement Task

The patient performs a series of movements to reach overhead and behind their back.

4. Flip objects

This tasks involves pronation and supination to flip objects.

5. Eating

The patient performs common eating motions such as cutting, securing, and scooping while simulating eating.

6. Insert objects into wells

[Supplementary figure VII: The Vivistim IPG.]
This task requires the patient to pick up small objects and place them in jars using the thumb and at least one additional digit.

7. Open and close a bottle or jar

The patient opens and closes various jars and bottles using finger dexterity and/or wrist motions.

In addition, participants performed additional (at least one) tasks. One example was fastening and unfastening a belt buckle.

**Long-Term Follow-Up and Post Implantation Care in VNS Group**

Participants were able to choose to have the device removed at any point during the study or to enter a long-term phase and receive further treatment at 6 monthly intervals. In the event of removal, both the generator and the portion of the lead up to the electrode would be removed. The electrode would likely also be removed, unless in the opinion of the surgeon, after viewing the electrode and nerve, removal of the electrode would convey a risk of nerve damage.
**Supplementary Results**

Supplementary Table I

<table>
<thead>
<tr>
<th>MRI Variable</th>
<th>VNS Group (n=9)</th>
<th>Rehabilitation Only Group (n=10)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Infarct volume, mm$^3$</td>
<td>85706.8 (76191.27)</td>
<td>55614.87 (86028.24)</td>
</tr>
<tr>
<td>Lesion to CST overlap volume, mm$^3$</td>
<td>8708.89 (5522.34)</td>
<td>5735.07 (5929.89)</td>
</tr>
<tr>
<td>CST FA ratio</td>
<td>0.72 (0.09)</td>
<td>0.81 (0.12)</td>
</tr>
<tr>
<td>MD ratio</td>
<td>1.45 (0.29)</td>
<td>1.28 (0.28)</td>
</tr>
</tbody>
</table>

Baseline MRI data by study group. MRI = magnetic resonance imaging. All values are mean (SD). CST = corticospinal tract. FA = fractional anisotropy. MD = mean diffusivity.
**Supplementary Table II**

<table>
<thead>
<tr>
<th></th>
<th>VNS Group (n=9)</th>
<th>Rehabilitation Only Group (n=10)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Infarct volume, mm³</td>
<td>r = 0.22, p=0.567</td>
<td>r = -0.16, p=0.663</td>
</tr>
<tr>
<td>Lesion to CST overlap volume, mm³</td>
<td>r = -0.03, p=0.936</td>
<td>r = -0.39, p=0.264</td>
</tr>
<tr>
<td>CST FA ratio</td>
<td>r = 0.19, p=0.631</td>
<td>r = 0.38, p=0.274</td>
</tr>
<tr>
<td>MD ratio</td>
<td>r = -0.02, p=0.967</td>
<td>r = -0.33, p=0.357</td>
</tr>
</tbody>
</table>

Correlation between change in FMA-UE score and baseline MRI variables in each study groups. Values shown are the Pearson correlation co-efficient and p value. CST = corticospinal tract. FA = fractional anisotropy. MD = mean diffusivity.
### Supplementary Table III

<table>
<thead>
<tr>
<th></th>
<th>VNS Responder (n=6)</th>
<th>Rehabilitation Only Responder (n=4)</th>
<th>P Value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Infarct Volume, mm³</td>
<td>109666 (79767)</td>
<td>3779 (3391)</td>
<td>0.023</td>
</tr>
<tr>
<td>Lesion to CST Overlap</td>
<td>1534 (1159)</td>
<td>1128 (1223)</td>
<td>0.036</td>
</tr>
<tr>
<td>FA ratio</td>
<td>0.79 (0.06)</td>
<td>0.85 (0.11)</td>
<td>0.014</td>
</tr>
<tr>
<td>MD ratio</td>
<td>1.39 (0.05)</td>
<td>1.17 (0.09)</td>
<td>0.034</td>
</tr>
</tbody>
</table>

Baseline MRI data in VNS treated responders compared to rehabilitation only responders. Response is defined as a > 6 point improvement in the FMA-UE score. Values shown are mean (SD). P values are for a 2-sample t test.